

US-PAT-NO: 5824040

DOCUMENT-IDENTIFIER: US 5824040 A

TITLE: Endoluminal prostheses and therapies
for highly variable
body lumens

----- KWIC -----

Detailed Description Text - DETX (22):

A method of fabricating a helical stent-graft 71 will be described with reference to FIG. 5E. A series of linked diamond-shaped elements 73 are first attached to a strip of liner material 75, typically being stitched with a sewing machine. The ribbon is then wound over a mandrel 77 of the desired size, and adjacent edges of the ribbon are sewn to each other (or otherwise permanently joined). Such a method may be substantially automated and continuous, and is thus particularly beneficial for producing a large number of prostheses. The helical stent-graft may optionally be cut to length, but will preferably include a crown stitched stent-ring 79 for sealing and ends against a surrounding lumen when deployed therein.

L Number	Hits	Search Text	DB	Time stamp
1	0	(measure or measuring) with aneurysm and stent and restrict\$3 near3 (dilation or expansion or expand)	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 14:46
2	43	(measure or measuring) with aneurysm and stent	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 14:57
3	74	(623/903).CCLS.	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 15:26
4	385	(623/1.13).CCLS.	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 15:46
5	118	(623/1.23).CCLS.	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 15:58
6	38	((measure or measuring) with aneurysm and stent) or ((623/903).CCLS.) or ((623/1.13).CCLS.) or ((623/1.23).CCLS.)) and (limit or limited) near3 expansion	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 16:13
7	992	623/1.15	USPAT; US-PGPUB; EPO; JPO; DERWENT	2003/09/05 16:14
8	47	("3304557" "3316557" "3945052" "4299015" "4652263" "4670286" "4731073" "4834755" "4922905" "5037377" "5064435" "5084065" "5123917" "5133742" "5163952" "5258042" "5282847" "5330500" "5387621" "5413598" "5443499" "5443500" "5456713" "5470313" "5476507" "5496364" "5507770" "5527353" "5545209" "5545210" "5556413" "5556426" "5562725" "5562727" "5591195" "5591199" "5609605" "5617878" "5683451" "5769882" "5824037" "5843158" "6019786" "6123722" "6176875" "6283991" "6361557").PN.	USPAT	2003/09/05 16:38

	Document ID	KSC	Issue	Pa	Title
1	US 6361557 B1	U	20020326	18	Staplebutton
2	US 6283991 B1	U	20010904	34	Endoluminal
3	US 6176875 B1	U	20010123	20	Limited expa
4	US 6123722 A	U	20000926	28	Stitched ste
5	US 6019786 A	U	20000201	19	Braided comp
6	US 5843158 A	U	19981201	21	Limited expa
7	US 5824037 A	U	19981020	28	Modular intr
8	US 5769882 A	U	19980623	19	Methods and
9	US 5683451 A	U	19971104	26	Apparatus an
10	US 5617878 A	U	19970408	15	Stent and me
11	US 5609605 A	U	19970311	8	Combination
12	US 5591199 A	U	19970107	8	Curable fi
13	US 5591195 A	U	19970107	18	Apparatus an
14	US 5562727 A	U	19961008	7	Intraluminal
15	US 5562725 A	U	19961008	10	Radially sel
16	US 5556426 A	U	19960917	11	PTFE implant
17	US 5556413 A	U	19960917	19	Coiled stent
18	US 5545210 A	U	19960813	7	Method of im
19	US 5545209 A	U	19960813	28	Controlled d
20	US 5527353 A	U	19960618	7	Implantable
21	US 5507770 A	U	19960416	7	Intraluminal
22	US 5496364 A	U	19960305	13	Self-support
23	US 5476507 A	U	19951219	12	Vascular pro
24	US 5470313 A	U	19951128	10	Variable dia
25	US 5456713 A	U	19951010	19	Expandable t
26	US 5443500 A	U	19950822	6	Intravascula
27	US 5443499 A	U	19950822	11	Radially exp
28	US 5413598 A	U	19950509	5	Vascular gra
29	US 5387621 A	U	19950207	8	Porous membr
30	US 5330500 A	U	19940719	8	Self-expandi
31	US 5282847 A	U	19940201	6	Prosthetic v
32	US 5258042 A	U	19931102	9	Intravascula
33	US 5163952 A	U	19921117	9	Expandable p
34	US 5133742 A	U	19920728	11	Crack-resist
35	US 5123917 A	U	19920623	9	Expandable i
36	US 5084065 A	U	19920128	7	Reinforced c
37	US 5064435 A	U	19911112	9	Self-expandi
38	US 5037377 A	U	19910806	6	Means for im
39	US 4922905 A	U	19900508	12	Dilatation c
40	US 4834755 A	U	19890530	11	Triaxially-b
41	US 4731073 A	U	19880315	11	Arterial gra
42	US 4670286 A	U	19870602	12	Method of fo
43	US 4652263 A	U	19870324	7	Elasticizati
44	US 4299015 A	U	19811110	8	Process for
45	US 3945052 A	U	19760323	5	Synthetic va
46	US 3316557 A	U	19670502	7	TEXT NOT AVA
47	US 3304557 A	U	19670221	7	TEXT NOT AVA

United States Patent (19)

Lam

(11) Patent Number: 5,556,413
(43) Date of Patent: Sep. 17, 1996

[54] COILED STENT WITH LOCKING ENDS

[75] Inventor: Sharon Lam, San Jose, Calif.
[73] Assignee: Advanced Cardiovascular Systems, Inc., Santa Clara, Calif.

[21] Appl. No.: 209,827

[22] Filed: Mar. 11, 1994

[51] Int. Cl.⁶ A61M 29/00

[52] U.S. Cl. 606/198; 623/1; 623/11

[58] Field of Search 606/200, 108, 104, 105; 623/1, 12; 128/896

[56] References Cited

U.S. PATENT DOCUMENTS

3,627,744 4/1972 Erick.
4,512,338 4/1983 Balho et al.
4,523,545 11/1983 Masas et al.
4,560,374 12/1983 Himmelfarb.
4,580,568 4/1986 Glasner.
4,625,771 4/1987 Wallick.
4,733,655 3/1988 Palmer.
4,739,762 4/1988 Palmer.
4,740,257 4/1988 Krummer.
4,762,124 8/1988 Rosenbluth.
4,776,337 10/1988 Palmer.
4,795,455 3/1989 Rogas.
4,800,882 1/1989 Glasner.
4,830,003 5/1989 Wolff et al.
4,854,516 8/1989 Himmelfarb.
4,877,020 10/1989 Beck et al.
4,878,395 11/1989 Lindemann et al.
4,886,662 12/1989 Wilner.
4,893,623 1/1990 Rosenbluth.
4,927,336 3/1990 Glasner.
5,133,141 4/1990 Himmelfarb.
4,927,905 5/1990 Siroder.
4,930,227 6/1990 Smith et al.
4,963,456 11/1990 Wilner.
4,965,890 11/1990 Sugita et al.
4,986,631 1/1991 King et al.
4,994,071 2/1991 MacGregor.
4,995,559 3/1991 Delaney.

(List continued on next page.)

FOREIGN PATENT DOCUMENTS

0382014 8/1990 European Pat. Off. 623/1
0408245A1 1/1991 European Pat. Off. 623/1
0501443 5/1992 European Pat. Off. 623/1
364245A1 6/1987 Germany.
2135583 9/1984 United Kingdom.
W0581843 9/1989 WIPO.

OTHER PUBLICATIONS

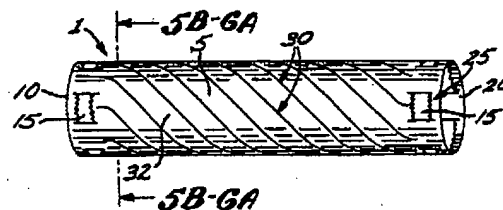
Wright et al.: Percutaneous Endovascular Stents: An Experimental Evaluation, 69-72, 1983, *Radiology Journal*.
Doser: Transluminal Expandable Nitinol Coil Stent Grafting: Preliminary Report, pp. 239-260, Apr. 1983, *Radiology Journal*.
Cragg et al.: Non-Surgical Placement of Arterial Endoprostheses: A New Technique Using Nitinol Wire, pp. 261-263, Apr. 1983, *Radiology Journal*.
Doser, Charles T.: Transluminally Placed Coil Spring Endarterial Tube Grafts, pp. 329-332, Oct. 1989, *Investigative Radiology*.
C. R. Bard PE Plus Peripheral Balloon Dilation Catheters, Aug. 1985, *CR Bard, Inc.*
Dupret et al.: Flexible Balloon-Expanded Stent for Small Vessels, pp. 276-278, 1987, *Radiology Journal*.
Masas et al.: Radiological Follow-up of Transluminally Inserted Vascular Endoprostheses: An Experimental Study Using Expanding Spirals, pp. 659-663, 1984, *Radiology Journal*.
Palmer et al.: Expandable Intraluminal Graft: A Preliminary Study, pp. 73-77, 1985, *Radiology Journal*.

Primary Examiner—Gary Jackson
Assistant Examiner—William W. Lewis
Attorney, Agent, or Firm—Fulwider Patton Lee & Utecht

[57] ABSTRACT

An intravascular stent comprising a cylindrical body capable of expansion having end assemblies capable of locking in an expanded state. The end assemblies may have a series of tabs and apertures that interlock and rotate as the stent ends expand to an open position to support a section of vasculature or other body lumen. The stent is bio-compatible, may be bio-erodible, and capable of localized drug delivery.

27 Claims, 9 Drawing Sheets



File Edit View Tools Window Help

	Document ID	Class	Issue-Date	Page	Title
1	US 3096560 A	U	19630709	5	TEXT NO
2	US 4140126 A	U	19790220	4	Method f
3	US 4182339 A	U	19800108	4	Anastomo
4	US 4501263 A	U	19850226	5	Method f
5	US 4546499 A	U	19851015	13	Method c
6	US 4623347 A	U	19861118	7	Antithro
7	US 5108407 A	U	19920428	10	Method c
8	US 5211683 A	U	19930518	33	Method c
9	US 5258020 A	U	19931102	9	Method c
10	US 5304220 A	U	19940419	38	Method c
11	US 5397345 A	U	19950318	17	Artifici
12	US 5407432 A	U	19950418	7	Method c
13	US 5413560 A	U	19950509	8	Method c
14	US 5425765 A	U	19950620	4	Surgical
15	US 5522880 A	U	19960604	12	Method f
16	US 5545210 A	U	19960813	7	Method c
17	US 5571172 A	U	19961105	19	Method c
18	US 5571169 A	U	19961105	21	Anti-ste
19	US 5571167 A	U	19961105	37	Bypass c
20	US 5575815 A	U	19961119	19	Local po
21	US 5591228 A	U	19970107	27	Methods
22	US 5593434 A	U	19970114	6	Stent ca
23	US 5609627 A	U	19970311	36	Method f
24	US 5609625 A	U	19970311	14	Endovasc
25	US 5653748 A	U	19970805	10	Device v
26	US 5653746 A	U	19970805	11	Radially
27	US 5662700 A	U	19970902	14	Artifici
28	US 5713859 A	U	19980203	10	Implanta
29	US 5755772 A	U	19980526	15	Radially
30	US 5766239 A	U	19980616	7	Balloon
31	US 5769885 A	U	19980623	33	Bifurcat
32	US 5782907 A	U	19980721	18	Involut
33	US 5782847 A	U	19980721	21	Anti-ste
34	US 5824034 A	U	19981020	9	Method f
35	US 5868780 A	U	19990209	6	Stents f
36	US 5916234 A	U	19990629	11	Expandab
37	US 5925076 A	U	19990720	65	Applianc
38	US 5931842 A	U	19990803	12	Methods
39	US 5938696 A	U	19990817	37	Bifurcat
40	US 5944019 A	U	19990831	38	Closed c
41	US 5980570 A	U	19991109	6	System c
42	US 5979455 A	U	19991109	38	Method f
43	US 6059821 A	U	20000509	11	Method f
44	US 6099557 A	U	20000808	6	Implanta
45	US 6132459 A	U	20001017	15	Method f
46	US 6156062 A	U	20001205	14	Helical
47	US 6186942 B1	U	20010213	32	Medical
48	US 6190397 B1	U	20010220	55	Means ar
49	US 6206912 B1	U	20010327	39	Medical
50	US 20010011189	U	20010802	57	In situ
51	US 20010025195	U	20010927	44	Flexible

United States Patent [19]

Lazarus

US005397345A
 [11] Patent Number: 5,397,345
 [45] Date of Patent: Mar. 14, 1995

- [54] ARTIFICIAL GRAFT AND IMPLANTATION METHOD
- [75] Inventor: Harrison M. Lazarus, Salt Lake City, Utah
- [73] Assignee: EndoVascular Technologies, Inc., Menlo Park, Calif.
- [21] Appl. No.: 175,491
- [22] Filed: Dec. 29, 1993

0423916 1/1990 European Pat. Off.
 0461791A1 12/1991 European Pat. Off.
 (List continued on next page.)

OTHER PUBLICATIONS

Alexander Balko, M.D., et al., Journal of Surgical Research 40: 305-309 (1986) "Transfemoral Placement of Intraluminal Polyurethane Prostheses for Abdominal Aortic Aneurysm".

David D. Lawrence, Jr., M.D., et al., Radiology 337-360 (1987). "Percutaneous Endovascular Graft: Experimental Evaluation".

(List continued on next page.)

Primary Examiner—Randall L. Green
 Assistant Examiner—Elizabeth M. Burke
 Attorney Agent or Firm—Folwider, Patton, Lee & Utecht

ABSTRACT

An intraluminal grafting system includes a hollow graft which has a proximal staple positioned proximate its proximal end and a distal staple adapted proximate its distal end. The system includes a capsule for transporting the graft through the lumen and for positioning the proximal end of the graft upstream in a lumen which may be a blood vessel or artery. A tube is connected to the capsule and extends to exterior the vessel for manipulation by the user. A catheter is positioned within the tube to extend from the cavity and through the graft to exterior the body. The catheter has an inflatable membrane or balloon proximate the distal end thereof which is in communication via a channel with inflation and deflation means located exterior the vessel. With the inflatable membrane deflated, the capsule is positioned in the lumen and manipulated to a desired location. The inflatable membrane is manipulated by the rod away from the graft. The force exerted by the inflatable membrane and the structure of the staples urges the staples in the vessel wall, retaining the graft in position. The remainder of the intraluminal grafting system is then removed from the corporeal vessel.

Related U.S. Application Data

- [60] Continuation of Ser. No. 34,587, Mar. 22, 1993, abandoned, which is a continuation of Ser. No. 732,058, Aug. 29, 1991, abandoned, which is a division of Ser. No. 166,059, Mar. 9, 1988, Pat. No. 5,104,399, which is a continuation-in-part of Ser. No. 946,507, Dec. 10, 1986, Pat. No. 4,787,839, which is a continuation of Ser. No. 359,933, Dec. 9, 1983, abandoned.

- [51] Int. Cl.⁶ A61F 2/06; A61F 2/54; A61B 17/00; A61B 29/00
- [52] U.S. Cl. 623/1; 606/153; 606/194; 604/95; 623/66
- [58] Field of Search 604/96, 104; 606/153, 606/158, 191, 192, 194, 195; 623/1, 2, 11, 66

References Cited

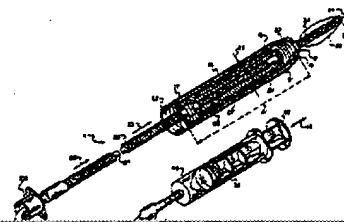
U.S. PATENT DOCUMENTS

- 5,334,629 11/1994 Cohn .
- 1,494,006 2/1970 Brunlik .
- 5,540,431 11/1970 Mohan-Uddin .
- 1,657,744 4/1972 Brink . 2/1
- 3,834,394 9/1974 Hunter et al. .
- 3,874,348 4/1975 King et al. .
- 3,908,662 9/1975 Ruzgic et al. .
- 3,938,499 2/1976 Buccio .
- 3,938,528 2/1976 Buccio .
- 4,025,747 2/1977 Kronenthal et al. .
- 4,047,232 9/1977 Leigh et al. .
- 4,056,534 11/1977 Barston et al. .
- 4,142,126 2/1979 Choudhury . 623/1 X
- (List continued on next page.)

FOREIGN PATENT DOCUMENTS

- 0150281 11/1984 European Pat. Off. .

10 Claims, 3 Drawing Sheets



File Edit View Tools Window Help

	Document ID	RSC	Issue-Date	Page	Title
1	US 3096560 A	U	19630709	5	TEXT NO
2	US 4140126 A	U	19790220	4	Method f
3	US 4182339 A	U	19800108	4	Anastomo
4	US 4501263 A	U	19850226	5	Method f
5	US 4546499 A	U	19851015	13	Method c
6	US 4623347 A	U	19861118	7	Antithro
7	US 5108407 A	U	19920428	10	Method c
8	US 5211683 A	U	19930518	33	Method c
9	US 5258020 A	U	19931102	9	Method c
10	US 5304220 A	U	19940419	38	Method c
11	US 5397345 A	U	19950314	17	Artifici
12	US 5407432 A	U	19950418	7	Method c
13	US 5413560 A	U	19950509	8	Method c
14	US 5425765 A	U	19950620	4	Surgical
15	US 5522880 A	U	19960604	12	Method f
16	US 5545210 A	U	19960813	7	Method c
17	US 5571172 A	U	19961105	19	Method c
18	US 5571169 A	U	19961105	21	Anti-ste
19	US 5571167 A	U	19961105	37	Bypass c
20	US 5575815 A	U	19961119	19	Local po
21	US 5591228 A	U	19970107	27	Methods
22	US 5593434 A	U	19970114	6	Stent, c
23	US 5609627 A	U	19970311	36	Method f
24	US 5609625 A	U	19970311	14	Endovasc
25	US 5653748 A	U	19970805	10	Device v
26	US 5653746 A	U	19970805	11	Radially
27	US 5662700 A	U	19970902	14	Artifici
28	US 5713859 A	U	19980203	10	Implanta
29	US 5755772 A	U	19980526	15	Radially
30	US 5766239 A	U	19980616	7	Balloon-
31	US 5769885 A	U	19980623	33	Bifurcat
32	US 5782907 A	U	19980721	18	Involute
33	US 5782847 A	U	19980721	21	Anti-ste
34	US 5824034 A	U	19981020	9	Method f
35	US 5868780 A	U	19990209	6	Stents
36	US 5916234 A	U	19990629	11	Expandab
37	US 5925076 A	U	19990730	65	Applian
38	US 5931842 A	U	19990803	12	Methods
39	US 5938696 A	U	19990817	37	Bifurcat
40	US 5944019 A	U	19990831	38	Closed c
41	US 5980570 A	U	19991109	6	System c
42	US 5979455 A	U	19991109	38	Method f
43	US 6059821 A	U	20000509	11	Method f
44	US 6099557 A	U	20000808	6	Implanta
45	US 6132459 A	U	20001017	15	Method f
46	US 6156062 A	U	20001205	14	Helical
47	US 6186942 B1	U	20010213	32	Medical
48	US 6190397 B1	U	20010220	55	Means ar
49	US 6206912 B1	U	20010327	39	Medical
50	US 20010011189	U	20010802	57	In situ
51	US 20010025195	U	20010927	44	Flexible



US 5925076A

United States Patent [19]

Inoue

[11] Patent Number: 5,925,076

[45] Date of Patent: *Jul. 20, 1999

[54] APPLIANCE TO BE IMPLANTED, METHOD OF COLLAPSING THE APPLIANCE TO BE IMPLANTED AND METHOD OF USING THE APPLIANCE TO BE IMPLANTED

5,507,767 4/1994 Maeda et al.
5,554,181 9/1990 Das
5,607,445 5/1997 Summers
5,606,626 3/1997 Kerasse
5,693,069 12/1997 Inoue

FOREIGN PATENT DOCUMENTS

[76] Inventor: Kanji Inoue, 98-13, Miyazaki-cho
Shimogamo, Kyoto, Japan

[*] Notice: This patent is subject to a terminal disclaimer.

[21] Appl. No.: 08/898,427

[22] Filed: Jul. 22, 1997

Related U.S. Application Data

[62] Division of application No. 08/765,216, Jan. 3, 1997, Pat. No. 5,843,162

Foreign Application Priority Data

May 19, 1995 [JP] Japan PC119550972

[51] Int. Cl. A61F 2/36

[52] U.S. Cl. 623/1; 623/12; 606/105; 606/138

[58] Field of Search 623/1; 11; 12; 606/198, 195, 194, 191, 108

References Cited

U.S. PATENT DOCUMENTS

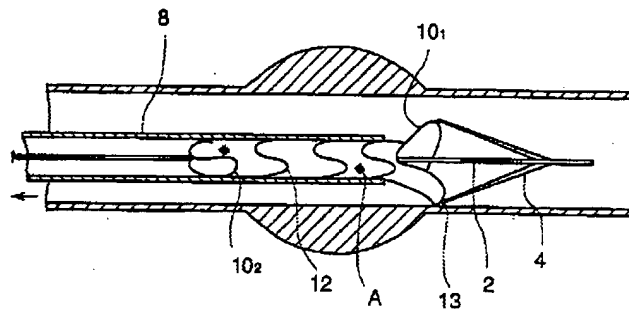
5,234,456 8/1993 Givens et al.
5,290,305 3/1994 Inoue
5,330,528 7/1994 Larkin
5,383,976 1/1995 Lock et al.
5,387,235 2/1995 Scott et al.

Primary Examiner—Paul B. Preblich
Assistant Examiner—Tam A. Nguyen
Attorney, Agent, or Firm—Barnes & Wozniak, Ltd.

[57] ABSTRACT

A collapsible artificial blood vessel A comprises a flexible front end wire ring 10₁, a flexible rear end wire ring 10₂ arranged facing to the front end wire ring, a tubular cover 7 which connects the end wire rings, and a plurality of intermediate wire rings 12 arranged spaced apart from each other between the front end wire ring and the rear end wire ring. The circumference of the front end wire ring is equally divided into four segments by dividing points 411, 421, 431, 441. Hooks 13 are formed for a front pull suture to be passed through at the dividing points 411, 431. The circumference of the intermediate wire rings are fixed to the tubular cover 7 by suturing or with adhesive at the positions 512, 523, 533 and 543. The device is collapsed for use by folding the wire rings and insertion of the device into a funnel tube.

6 Claims, 49 Drawing Sheets



	Document ID	KS	Issue	Dr	Page	Title
51	US 20030078647	U	20030424	10	Andioplasty	
52	US 6551350 B1	U	20030422	44	Kink resist	
53	US 20030074050	U	20030417	28	Stent/graft	
54	US 20030074049	U	20030417	30	Covered st	
55	US 20030074048	U	20030417	9	Tubular pr	
56	US 6547815 B2	U	20030415	10	Intralumin	
57	US 6547814 B2	U	20030415	16	Selective	
58	US 20030065380	U	20030403	18	Endovascu	
59	US 20030065379	U	20030403	13	Reduction	
60	US 20030065378	U	20030403	11	Medical se	
61	US 20030065377	U	20030403	45	Coated med	
62	US 6540773 B2	U	20030401	21	Low profil	
63	US 6537310 B1	U	20030325	17	Endolumina	
64	US 20030055484	U	20030320	20	Exterior st	
65	US 6530950 B1	U	20030311	14	Intralumin	
66	US 20030045926	U	20030306	10	Self artic	
67	US 6524337 B1	U	20030225	6	Intralumin	
68	US 6524335 B1	U	20030225	14	Endolumina	
69	US 6524334 B1	U	20030225	12	Expandable	
70	US 6520986 B2	U	20030218	34	Kink resist	
71	US 20030033002	U	20030213	14	Aorto uni	
72	US 6517573 B1	U	20030211	10	Hook for a	
73	US 6517572 B2	U	20030211	39	Endovascu	
74	US 6517571 B1	U	20030211	25	Vascular g	
75	US 6517570 B1	U	20030211	22	Exterior st	
76	US 20030028246	U	20030206	15	Compliant	
77	US 20030028240	U	20030206	16	Stent-graft	
78	US 20030028239	U	20030206	22	LOW PROFIL	
79	US 6514283 B2	U	20030204	10	Intralumin	
80	US 6514282 B1	U	20030204	35	Method of	
81	US 20030023300	U	20030130	16	Endolumina	
82	US 20030023299	U	20030130	16	Reposition	
83	US 6511505 B2	U	20030128	16	Variable st	
84	US 20030018378	U	20030123	16	Endovascu	
85	US 6508835 B1	U	20030121	37	Endolumina	
86	US 20030009213	U	20030109	12	Stent hav	
87	US 20030009212	U	20030109	20	Axially-co	
88	US 20030009211	U	20030109	17	Implant hav	
89	US 20030009210	U	20030109	11	ePTFE graft	
90	US 20030006528	U	20030109	16	Methods fo	
91	US 20030004562	U	20030102	13	Endolumina	
92	US 6500203 B1	U	20021231	25	Process fo	
93	US 20020198588	U	20021226	28	Covered end	
94	US 20020198587	U	20021226	19	Modular st	
95	US 20020198586	U	20021226	47	APPLIANCE	
96	US 6497722 B1	U	20021224	10	Methods and	
97	US 20020193864	U	20021219	18	Coiled she	
98	US 6494909 B2	U	20021217	14	Endovascu	
99	US 6488701 B1	U	20021203	16	Stent-graft	
100	US 6485513 B1	U	20021126	10	Percutaneou	
101	US 20020173836	U	20021121	12	Method of	
102	US 6482227 B1	U	20021119	27	Stent graft	
103	US 20020169497	U	20021114	36	Endovascu	
104	US 20020169496	U	20021114	19	Methods for	
105	US 6478813 B1	U	20021112	37	Method for	
106	US 20020165603	U	20021107	40	Kink-resist	
107	US 20020165602	U	20021107	23	Self expand	



US 20020165603A1

(19) United States

(12) Patent Application Publication
Thornton et al.

(10) Pub. No.: US 2002/0165603 A1
(43) Pub. Date: Nov. 7, 2002

(54) KINK-RESISTANT BIFURCATED
PROSTHESIS

Publication Classification

(76) Inventors: Troy Thornton, San Francisco, CA
(US); Randy S. Chan, San Jose, CA
(US); Lilip Lau, Sunnyvale, CA (US)

(51) Int. Cl.⁷ A61F 2/06
(52) U.S. Cl. 623/1.13; 623/1.22; 623/1.35;
623/1.36

Correspondence Address:
MORGAN & FINNEGAN, L.L.P.
349 Park Avenue
New York, NY 10154-0053 (US)

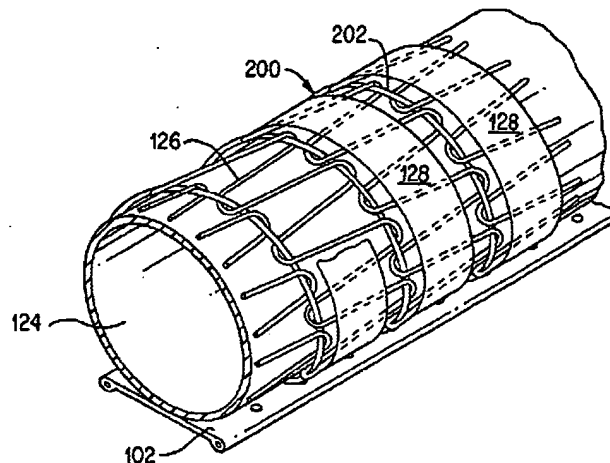
(57) ABSTRACT

(21) Appl. No.: 10/184,989
(22) Filed: Jul. 1, 2002

Related U.S. Application Data

(63) Continuation of application No. 08/772,372, filed on
Dec. 23, 1996.

The invention consists of an endoluminal prosthesis adapted for placement at a bifurcation site within the body. The stent or stent-graft may be constructed to have segments of differing structural properties. A section of the stent-graft may be constructed to have a single-lumen tubular stent member covering a multi-lumen graft member. The stent-graft may comprise at least two modular components adapted for in situ assembly. An extended cylindrical interference fit may be used to seal the modular components.



	Document ID	KS	Issue	Da	Page	Title
64	US 20030055484	U	20030320	20	Exterior s	
65	US 6530950 B1	U	20030311	14	Intralumin	
66	US 20030045926	U	20030306	10	Self artic	
67	US 6524337 B1	U	20030225	6	Intralumin	
68	US 6524335 B1	U	20030225	14	Endolumina	
69	US 6524334 B1	U	20030225	12	Expandable	
70	US 6520986 B2	U	20030218	34	Kink resist	
71	US 20030033002	U	20030213	14	Aorto uni-	
72	US 6517573 B1	U	20030211	10	Hook for a	
73	US 6517572 B2	U	20030211	39	Endovascu	
74	US 6517571 B1	U	20030211	25	Vascular g	
75	US 6517570 B1	U	20030211	22	Exterior s	
76	US 20030028246	U	20030206	15	Compliant	
77	US 20030028240	U	20030206	16	Stent-graft	
78	US 20030028239	U	20030206	22	LOW PROFILE	
79	US 6514283 B2	U	20030204	10	Intralumin	
80	US 6514282 B1	U	20030204	35	Method of	
81	US 20030023300	U	20030130	16	Endolumina	
82	US 20030023299	U	20030130	16	Reposition	
83	US 6511505 B2	U	20030128	16	Variable s	
84	US 20030018378	U	20030123	16	Endovascu	
85	US 6508835 B1	U	20030121	37	Endolumina	
86	US 20030009213	U	20030109	12	Stent havin	
87	US 20030009212	U	20030109	20	Axially-co	
88	US 20030009211	U	20030109	17	Implant hav	
89	US 20030009210	U	20030109	11	ePTFE graft	
90	US 20030006528	U	20030109	16	Methods for	
91	US 20030004562	U	20030102	13	Endolumina	
92	US 6500203 B1	U	20021231	25	Process for	
93	US 20020198588	U	20021226	28	Covered end	
94	US 20020198587	U	20021226	19	Modular st	
95	US 20020198586	U	20021226	47	APPLIANCE	
96	US 6497722 B1	U	20021224	10	Methods and	
97	US 20020193864	U	20021219	18	Coiled shee	
98	US 6494909 B2	U	20021217	14	Endovascu	
99	US 6488701 B1	U	20021203	16	Stent-graft	
100	US 6485513 B1	U	20021126	10	Percutaneou	
101	US 20020173836	U	20021121	12	Method of	
102	US 6482227 B1	U	20021119	27	Stent graft	
103	US 20020169497	U	20021114	36	Endovascu	
104	US 20020169496	U	20021114	19	Methods for	
105	US 6478813 B1	U	20021112	37	Method for	
106	US 20020165603	U	20021107	42	Kink-resist	
107	US 20020165602	U	20021107	23	Self expand	
108	US 20020165601	U	20021107	11	Bioabsorba	
109	US 6475232 B1	U	20021105	12	Stent with	
110	US 20020156523	U	20021024	22	Exterior s	
111	US 20020156522	U	20021024	10	Aortic gra	
112	US 20020156521	U	20021024	25	Bifurcated	
113	US 20020156518	U	20021024	15	Branched a	
114	US 6468301 B1	U	20021022	15	Reposition	
115	US 6468300 B1	U	20021022	5	Stent cover	
116	US 20020151958	U	20021017	14	Large vesse	
117	US 20020151957	U	20021017	20	Axially-co	
118	US 6464719 B2	U	20021015	6	Low profile	
119	US 20020147492	U	20021010	22	Endolumina	
120	US 6461320 B1	U	20021008	34	Method and	



US 20020147492A1

(19) United States

(12) Patent Application Publication
Shokoochi et al.

(10) Pub. No.: US 2002/0147492 A1
(43) Pub. Date: Oct. 10, 2002

(34) ENDOLUMINAL VASCULAR PROSTHESIS

Related U.S. Application Data

(76) Inventors: Mehrdad M. Shokoochi, Rancho Palos Verdes, CA (US); Michael R. Henson, Trabuco Canyon, CA (US); Gerard von Hoffmann, Trabuco Canyon, CA (US)

(53) Continuation of application No. 09/483,411, filed on Jan. 14, 2000, now Pat. No. 6,331,190, which is a continuation of application No. 09/034,689, filed on Mar. 4, 1998, now Pat. No. 6,077,296.

Publication Classification

Correspondence Address:
KNOBBE MARTENS OLSON & BEAR LLP
620 NEWPORT CENTER DRIVE
SIXTEENTH FLOOR
NEWPORT BEACH, CA 92660 (US)

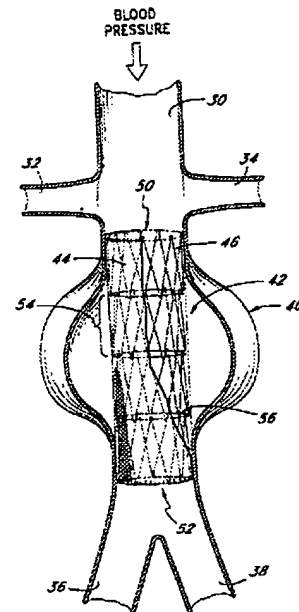
(51) Int. Cl.⁷ A61F 2/06
(52) U.S. Cl. 623/1.13; 623/1.16

(57) ABSTRACT

Disclosed is a tubular endoluminal vascular prosthesis, useful in treating, for example, an abdominal aortic aneurysm. The prosthesis comprises a self expandable wire support structure surrounded by a flexible tubular membrane. A delivery catheter and methods are also disclosed.

(21) Appl. No.: 10/032,230

(22) Filed: Dec. 18, 2001



	Document ID	KS	Issue	Da	Page	Title
124	US 6451051 B2	U	20020917	100	Intravascu	
125	US 6451048 B1	U	20020917	25	Wire connec	
126	US 6451047 B2	U	20020917	16	Encapsulat	
127	US 20020128703	U	20020912	8	METHOD AND	
128	US 20020123789	U	20020905	10	Stent cover	
129	US 20020123788	U	20020905	10	Sheath for	
130	US 6443981 B1	U	20020903	12	Expandable	
131	US 20020116048	U	20020822	16	Endovascu	
132	US 6436132 B1	U	20020820	10	Composite	
133	US 20020111668	U	20020815	9	Seamless b	
134	US 20020111667	U	20020815	14	Non-expand	
135	US 6432131 B1	U	20020813	8	Method and	
136	US 20020107565	U	20020808	15	Endovascu	
137	US 6428550 B1	U	20020806	34	Sutureless	
138	US 20020103527	U	20020801	13	Stent with	
139	US 20020095205	U	20020718	7	Encapsulat	
140	US 20020095140	U	20020718	15	Reposition	
141	US 20020091437	U	20020711	12	Polymer co	
142	US 6416537 B1	U	20020709	7	Multi-stage	
143	US 20020082675	U	20020627	10	Intralumin	
144	US 20020082674	U	20020627	9	Surgical g	
145	US 20020077693	U	20020620	21	Covered, co	
146	US 20020068967	U	20020606	104	Intravascu	
147	US 6398803 B1	U	20020604	7	Partial enc	
148	US 6398802 B1	U	20020604	15	Low profile	
149	US 20020065546	U	20020530	14	Stent graft	
150	US 6395022 B1	U	20020528	13	Endovascu	
151	US 6395019 B2	U	20020528	20	Endovascu	
152	US 6395018 B1	U	20020528	21	Endovascu	
153	US 20020062147	U	20020523	17	Stent havi	
154	US 20020062146	U	20020523	38	Methods and	
155	US 6390098 B1	U	20020521	25	Percutaneo	
156	US 20020058993	U	20020516	37	Supra-rena	
157	US 20020058987	U	20020516	33	Bilateral	
158	US 20020058986	U	20020516	33	Stent graft	
159	US 20020058985	U	20020516	22	Thoracic a	
160	US 20020058984	U	20020516	28	Extension	
161	US 20020055769	U	20020509	13	Stent with	
162	US 20020055768	U	20020509	13	METHOD OF	
163	US 6383214 B1	U	20020507	15	Encapsulat	
164	US 6383171 B1	U	20020507	36	Methods and	
165	US 20020052645	U	20020502	18	Endovascu	
166	US 20020052644	U	20020502	46	Implantabl	
167	US 20020052643	U	20020502	22	Tapered enc	
168	US 6379382 B1	U	20020430	10	Stent havi	
169	US 20020049489	U	20020425	7	Prosthesis	
170	US 6375675 B2	U	20020423	48	Methods and	
171	US 20020045931	U	20020418	10	Support str	
172	US 6371982 B2	U	20020416	11	Graft struc	
173	US 6371981 B1	U	20020416	14	Vascular g	
174	US 20020042646	U	20020411	7	Stent devic	
175	US 20020042645	U	20020411	27	Drug eluti	
176	US 20020042644	U	20020411	11	Bifurcated	
177	US 6368345 B1	U	20020409	49	Methods and	
178	US 20020040237	U	20020404	9	ePTFE graf	
179	US 20020040236	U	20020404	27	PROCEDURES	
180	US 20020040235	U	20020404	11	Endovascu	



(19) United States
(12) Patent Application Publication (10) Pub. No.: US 2002/0040236 A1
LAU et al. (43) Pub. Date: Apr. 4, 2002

(54) PROCEDURES FOR INTRODUCING STENTS AND STENT-GRAFTS (52) U.S. Cl. 623/1.12; 623/1.13; 623/1.17; 623/1.2; 623/1.23

(75) Inventors: LILIP LAU, SUNNYVALE, CA (US); CHARLES T. MARONEY, PORTOLA VALLEY, CA (US); WILLIAM M. HARTIGAN, FREMONT, CA (US); SHARON LAM, SAN JOSE, CA (US)

Correspondence Address:
MICHAEL S. MARCUS
MORGAN & FINNEGAN, LLP
345 PARK AVENUE
NEW YORK, NY 10154

(73) Assignee: Gore Enterprise Holdings, Inc.

(*) Notice: This is a publication of a continued prosecution application (CPA) filed under 37 CFR 1.53(d).

(21) Appl. No.: 08/896,373

(22) Filed: Jul. 18, 1997

Related U.S. Application Data

(63) Continuation of application No. 08/754,398, filed on Nov. 20, 1996, now abandoned.

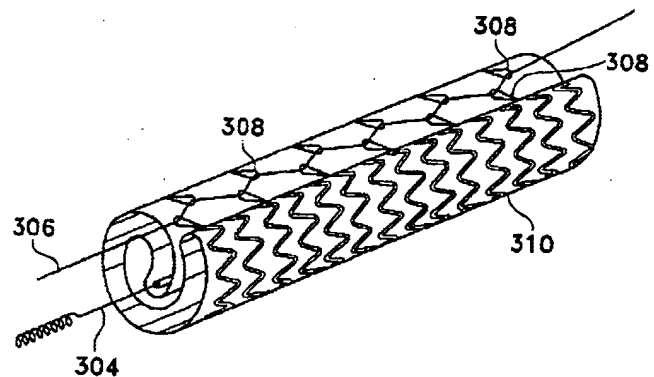
Publication Classification

(51) Int. Cl. A61F 2/06

(57) ABSTRACT

This invention is a medical device and a method of using it. The device is a foldable stent or stent-graft which may be percutaneously delivered with (or on) a catheter, typically an endovascular catheter, to a body cavity or lumen and then expanded. It may also be delivered or via surgical (or other) techniques. The expandable stent structure utilizes occasional members which distribute bending and folding loads in such a way that the stent is not plastically deformed. The stent's configuration allows it to be folded or otherwise compressed to a very small diameter prior to deployment without changing the length of the stent. The graft component cooperating with the stent is tubular and preferably is blood-compatible material which may, if desired, be reinforced with fibers. The stent is able to provide collapsible support for otherwise fragile graft material.

The invention also involves procedures for folding stents and for deploying stents or stent-grafts which have been folded, banded, or otherwise collapsed to significantly smaller diameters for insertion into a human or animal body. When used with super-elastic alloys, the stent may be collapsed at a convenient temperature either above or, preferably, below the transition temperature of the alloy. The deployment procedures may involve the use of an outer sleeve to maintain the stent or stent-graft at a reduced diameter; or may involve one or more external or internal "zip-lines" or "tether wires" to hold and then to release the device.



	Document ID	KS	Issue	Da	Page	Title
186	US 6361557 B1	U	20020326	18	Staplebutt	
187	US 20020035395	U	20020321	26	Implantable	
188	US 20020035394	U	20020321	23	Methods and	
189	US 6357104 B1	U	20020319	9	Method of	
190	US 20020032487	U	20020314	17	Prosthesis	
191	US 6355056 B1	U	20020312	8	Implantable	
192	US 6355055 B1	U	20020312	8	Endovascu	
193	US 20020026231	U	20020228	16	Radially ex	
194	US 20020026230	U	20020228	27	Removable	
195	US 20020026137	U	20020228	31	Method and	
196	US 20020019665	U	20020214	48	Methods and	
197	US 6346119 B1	U	20020212	8	Graft equi	
198	US 20020016627	U	20020207	13	Tubular st	
199	US 20020016626	U	20020207	10	Intralumin	
200	US 20020016625	U	20020207	12	Drug/drug	
201	US 6344054 B1	U	20020205	7	Endolumina	
202	US 6340366 B1	U	20020122	15	Stent with	
203	US 20020007208	U	20020117	11	Device with	
204	US 20020004677	U	20020110	6	Low profile	
205	US 6336937 B1	U	20020108	27	Multi-stage	
206	US 6334869 B1	U	20020101	25	Endolumina	
207	US 6334868 B1	U	20020101	6	Stent cover	
208	US 6334867 B1	U	20020101	7	Surgical g	
209	US 20010053930	U	20011220	41	Endovascu	
210	US 6331527 B1	U	20011218	69	Promoter st	
211	US 6331188 B1	U	20011218	22	Exterior st	
212	US 20010049550	U	20011206	31	METHOD OF	
213	US 6325820 B1	U	20011204	14	Coiled-she	
214	US 20010047198	U	20011129	104	Intravascu	
215	US 20010044647	U	20011122	13	Modular enc	
216	US 6319278 B1	U	20011120	9	Low profile	
217	US 6319277 B1	U	20011120	10	Nested ste	
218	US 20010041928	U	20011115	7	Endovascu	
219	US 20010041927	U	20011115	7	By-pass dr	
220	US 6315792 B1	U	20011113	34	Remotely re	
221	US 6315791 B1	U	20011113	15	Self-expans	
222	US 20010039446	U	20011108	20	ENCAPSULAT	
223	US 6312458 B1	U	20011106	14	Tubular st	
224	US 6312457 B1	U	20011106	10	Intralumin	
225	US 6312456 B1	U	20011106	7	Biocompatil	
226	US 20010037142	U	20011101	16	Endovascu	
227	US 20010037139	U	20011101	31	Method and	
228	US 6309413 B1	U	20011030	12	Expandable	
229	US 6309343 B1	U	20011030	9	Method for	
230	US 20010032009	U	20011018	7	Partial enc	
231	US 20010027338	U	20011004	11	Endovascu	
232	US 6296661 B1	U	20011002	21	Self-expans	
233	US 20010025195	U	20010927	44	Flexible v	
234	US 20010025131	U	20010927	13	Methods fo	
235	US 6293965 B1	U	20010925	24	Tubular mec	
236	US 20010023370	U	20010920	12	COMPOSITE	
237	US 6290720 B1	U	20010918	13	Stretchable	
238	US 20010021870	U	20010913	13	Externally	
239	US 6287330 B1	U	20010911	37	Aortoiliac	
240	US 20010020182	U	20010906	26	Expandable	
241	US 20010020181	U	20010906	7	PARTIAL EN	
242	US 6292801 B1	U	20010904	34	Endolumina	



US 20010020181A1

(19) United States

(12) Patent Application Publication
LAYNE

(10) Pub. No.: US 2001/0020181 A1
(43) Pub. Date: Sep. 6, 2001

(54) PARTIAL ENCAPSULATION OF STENTS
USING STRIPS AND BANDS

(52) U.S. Cl. 623/1.13; 623/1.16; 623/1.49

(76) Inventor: RICHARD LAYNE, PHOENIX, AZ
(US)

(57) ABSTRACT

Correspondence Address:
MORRISON & FOERSTER LLP
555 WEST FIFTH STREET SUITE 3500
LOS ANGELES, CA 90013-1024 (US)

(*) Notice: This is a publication of a continued prosecution application (CPA) filed under 37 CFR 1.53(d).

(21) Appl. No.: 09/408,890

(22) Filed: Sep. 29, 1999

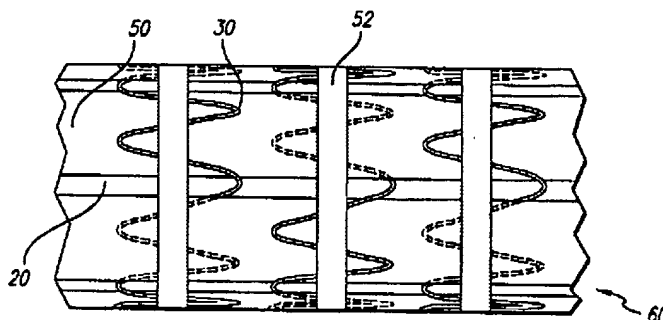
Related U.S. Application Data

(63) Non-provisional of provisional application No. 60/118,269, filed on Feb. 2, 1999.

Publication Classification

(51) Int. Cl. A61F 2/06

Partially encapsulated stents are made using strips and bands of covering material. In one embodiment: ringed stents are placed over an inner ePTFE tube (e.g., supported on a mandrel) and are covered by a series of longitudinal strips. A series of spaced apart ePTFE circumferential bands can then be placed over the top of the longitudinal strips and ringed stents; alternatively bands alone or strips alone may be employed. All of the components of the structure are then laminated to the inner ePTFE tube to capture the stent. By selecting the size and position of the ePTFE bands, it is possible to leave critical parts of the stent unencapsulated to facilitate flexibility and expansion. The longitudinal strips can be woven about the stent and later laminated into position to provide an anti-compression function as well as overall structural stability. Although a single stent can be used, these approaches lend themselves to use of a plurality of individual ring stents spaced apart along the inner ePTFE tube.



EAST Browser L6: (38) (2 or 3 or 4) [US 5443499 A] Tag: S [Doc: 2/38 (SORTED)] Format: KWIC						
File	Edit	View	Tools	Window	Help	
	Document ID	Issue	Date	Page	Title	
1	US 5123917 A	U	19920623	9	Expandab	US-PAT-NO: 5443499
2	US 5443499 A	U	19960822	11	Radially	DOCUMENT-IDENTIFIER: US 5443499 A
3	US 5653746 A	U	19970805	11	Radially	TITLE: Radially expandable tubular prosthesis
4	US 5728131 A	U	19980317	11	Coupling	----- KWIC -----
5	US 5782904 A	U	19980721	9	Intralum	Brief Summary Text - BSTX (10):
6	US 5824046 A	U	19981020	14	Covered	In one preferred embodiment, the prosthesis is made from a woven fabric
7	US 5824042 A	U	19981020	23	Endolumi	having substantially drawn longitudinal yarns (warp yarns) which
8	US 5824037 A	U	19981020	28	Modular	expansion or elongation of the prosthesis in the longitudinal direction, and
9	US 5824034 A	U	19981020	9	Method f	radial yarns (fill yarns) which are at most partially drawn to allow for
10	US 5843158 A	U	19981201	21	Limited	expansion of the prosthesis in the radial direction when the yield point of the
11	US 6036725 A	U	20000314	14	Expandab	radial yarns is exceeded.
12	US 6110198 A	U	20000829	27	Method f	Current US Cross Reference Classification - CCXR (1):
13	US 6139573 A	U	20001031	19	Conforma	6237113
14	US 6193745 B1	U	20010227	28	Modular	
15	US 6203568 B1	U	20010320	23	Endolumi	
16	US 20010000188	U	20010405	21	Limited	
17	US 6224625 B1	U	20010501	6	Low prof	
18	US 6245099 B1	U	20010612	16	Selectiv	
19	US 20010010012	U	20010726	17	Selectiv	
20	US 6270523 B1	U	20010807	13	Expandab	
21	US 20010044647	U	20011122	13	Modular	
22	US 6334868 B1	U	20020101	6	Stent co	
23	US 6336937 B1	U	20020108	27	Multi-st	
24	US 20020004677	U	20020110	6	Low prof	
25	US 6344054 B1	U	20020205	7	Endolumi	
26	US 20020045931	U	20020418	10	Support	
27	US 6416522 B1	U	20020709	17	Intralum	
28	US 6464719 B2	U	20021015	6	Low prof	
29	US 6475232 B1	U	20021105	12	Stent wi	
30	US 20020173837	U	20021121	19	Prosthet	
31	US 20030065379	U	20030403	13	Reductio	
32	US 6547814 B2	U	20030415	16	Selectiv	
33	US 6554855 B1	U	20030429	22	Low prof	
34	US 20030093145	U	20030515	20	Endolumi	
35	US 6565596 B1	U	20030520	11	Intralum	
36	US 20030125796	U	20030703	21	Low prof	
37	US 6592614 B2	U	20030715	20	Cuffed e	
38	US 20030149472	U	20030807	13	Modular	

US-PAT-NO: 5443499

DOCUMENT-IDENTIFIER: US 5443499 A

TITLE: Radially expandable tubular
prosthesis

----- KWIC -----

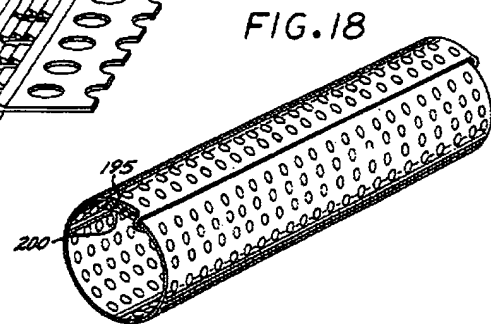
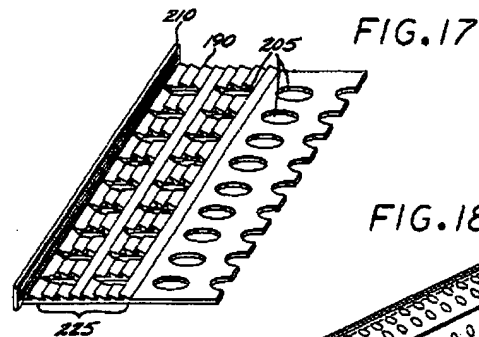
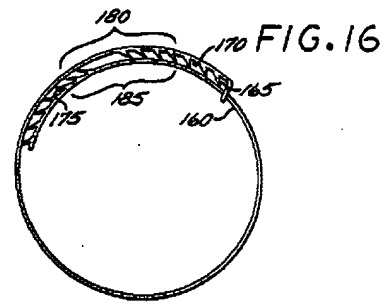
Brief Summary Text - BSTX (10):

In one preferred embodiment, the prosthesis is made from a woven fabric having substantially drawn longitudinal yarns (warp yarns) which limit expansion or elongation of the prosthesis in the longitudinal direction, and radial yarns (fill yarns) which are at most partially drawn to allow for expansion of the prosthesis in the radial direction when the yield point of the radial yarns is exceeded.

Current US Cross Reference Classification - CCXR (1):
623/1.13

EAST Browser L6 (38) (2 or 3 or 4) [US 5824037 A] Tag: S Doc: 8/38 (SORTED) Format: KWIC							
File Edit View Tools Window Help							
	Document ID	RSC	Issue-Date	Page	T		
1	US 5123917 A	U	19920623	9	Expan	US-PAT-NO: 5824037	
2	US 5443499 A	U	19950822	11	Radia	DOCUMENT-IDENTIFIER: US 5824037 A	
3	US 5653746 A	U	19970805	11	Radia	TITLE: Modular intraluminal prostheses construction and methods	
4	US 5728131 A	U	19980317	11	Coupl		
5	US 5782904 A	U	19980721	9	Intra		
6	US 5824046 A	U	19981020	14	Cover		
7	US 5824042 A	U	19981020	23	Endol		
8	US 5824037 A	U	19981020	28	Modul	----- KWIC -----	
9	US 5824034 A	U	19981020	9	Metho	Brief Summary Text - BSTX (23):	
10	US 5843158 A	U	19981201	21	Limit	In yet another aspect, the present invention provides a liner-limited	
11	US 6036725 A	U	20000314	14	Expan	stent-graft comprising a resilient radially expandable tubular frame, and a	
12	US 6110198 A	U	20000829	27	Metho	tubular liner disposed over at least a portion of an inner or outer surface of	
13	US 6139573 A	U	20001031	19	Confo	the frame. The liner limits the resilient expansion of at least a portion of	
14	US 6193745 B1	U	20010227	28	Modul	the frame when the stent-graft is in a relaxed state. Advantageously, when the	
15	US 6203568 B1	U	20010320	23	Endol	liner is disposed within the frame the tension from the frame provides a smooth	
16	US 20010000188	U	20010405	21	Limit	prosthetic lumen defined at least in part by a taut liner surface.	
17	US 6224625 B1	U	20010501	6	Low p	Furthermore, axial variations in the perimeter of the liner produce axial	
18	US 6245099 B1	U	20010612	16	Selec	variations in the stent-graft lumen, even where the frame structure remains	
19	US 20010010012	U	20010726	17	Selec	axially uniform in diameter. Such liner-limited stent-grafts are particularly	
20	US 6270523 B1	U	20010807	13	Expan	well-suited for use with the selective shrinking or plastic expansion of a	
21	US 20010044647	U	20011122	13	Modul	liner to produce axially tailored endoluminal prosthesis, as described	
22	US 6334868 B1	U	20020101	6	Stent	hereinbelow.	
23	US 6336937 B1	U	20020108	27	Multi	Detailed Description Text - DETX (27):	
24	US 200200004677	U	20020110	6	Low p	A third axially varying prosthesis 130 includes an inelastic inner flared	
25	US 6344054 B1	U	20020205	7	Endol	graft 132 which restrains the total diameter of the prosthesis from within the	
26	US 20020045931	U	20020418	10	Suppo	stent through the stent/graft attachment threads. The graft includes a greater	
27	US 6416522 B1	U	20020709	17	Intra	perimeter at both ends, allowing the stent rings located in the end portions to	
28	US 6464719 B2	U	20021015	6	Low p	expand to a larger diameter. The shape of this prosthesis is particularly well	
29	US 6475232 B1	U	20021105	12	Stent	suited for treatment of aneurysms and other weakened vessels, as the flared	
30	US 20020173837	U	20021121	19	Prost	ends provide secure proximal and distal anchors beyond the aneurysm, while the	
31	US 20030065379	U	20030403	13	Reduc	liner limits expansion of a central portion of the prosthesis to avoid	
32	US 6547814 B2	U	20030415	16	Selec	distressing the weakened vessel wall at the aneurysm itself.	
33	US 6554855 B1	U	20030429	22	Low p	Detailed Description Text - DETX (28):	
34	US 20030093145	U	20030515	20	Endol	Graft material is typically highly flexible so that the prosthesis is	
35	US 6565596 B1	U	20030520	11	Intra	radially compressible to a narrow diameter configuration for insertion and	
36	US 20030125796	U	20030703	21	Low p	positioning within a body lumen. However, the graft material is also generally	
37	US 6592614 B2	U	20030715	20	Cuffe	inelastic to avoid any stretching of the liner material after deployment, as	
38	US 20030149472	U	20030807	13	Modul	excess loose fabric may interfere with the flow through the prosthesis lumen.	

	Document ID	Class	Issue-Or	Page	Title
907	US 5800456 A	U	19980901	8	Spiral stent
908	US 5788626 A	U	19980804	12	Method of
909	US 5782906 A	U	19980721	8	Combination
910	US 5779732 A	U	19980714	8	Method and
911	US 5779729 A	U	19980714	4	Coated stent
912	US 5776183 A	U	19980707	7	Expandable
913	US 5776182 A	U	19980707	20	Blood control
914	US 5776181 A	U	19980707	21	Expandable
915	US 5766710 A	U	19980616	12	Biodegradable
916	US 5755782 A	U	19980526	16	Stents for
917	US 5755776 A	U	19980526	11	Permanent
918	US 5755771 A	U	19980526	10	Expandable
919	US 5741293 A	U	19980421	18	Locking stent
920	US 5735897 A	U	19980407	8	Intravascular
921	US 5733330 A	U	19980331	8	Balloon-expandable
922	US 5733303 A	U	19980331	14	Flexible endoprosthesis
923	US 5728150 A	U	19980317	15	Expandable
924	US 5725549 A	U	19980310	18	Coiled stent
925	US 5725548 A	U	19980310	5	Self-locking
926	US 5718713 A	U	19980217	10	Surgical stent
927	US 5716981 A	U	19980210	121	Anti-angiogenic
928	US 5700286 A	U	19971223	14	Polymer film
929	US 5697971 A	U	19971216	8	Multi-cell
930	US 5690670 A	U	19971125	17	Stents of
931	US 5674278 A	U	19971007	8	Endovascular
932	US 5672169 A	U	19970930	7	Stent mount
933	US 5653727 A	U	19970805	14	Intravascular
934	US 5649977 A	U	19970722	7	Metal reinforcement
935	US 5649952 A	U	19970722	10	Expandable
936	US 5643312 A	U	19970701	9	Stent having
937	US 5643309 A	U	19970701	13	Cardiovascular
938	US 5632840 A	U	19970527	7	Method of
939	US 5632771 A	U	19970527	17	Flexible stent
940	US 5632763 A	U	19970527	7	Bifurcated
941	US 5630840 A	U	19970520	12	Clad composite
942	US 5630829 A	U	19970520	14	High hoop stress
943	US 5629077 A	U	19970513	9	Biodegradable
944	US 5628787 A	U	19970513	10	Clad composite
945	US 5628785 A	U	19970513	14	Bioelastomer
946	US 5624411 A	U	19970429	13	Intravascular
947	US 5607468 A	U	19970304	7	Method of
948	US 5599352 A	U	19970204	15	Method of
949	US 5591227 A	U	19970107	14	Drug eluting
950	US 5591224 A	U	19970107	14	Bioelastomer
951	US 5591223 A	U	19970107	5	Re-expandable
952	US 5591222 A	U	19970107	9	Method of
953	US 5578075 A	U	19961126	11	Minimally
954	US 5575818 A	U	19961119	13	Endovascular
955	US 5575816 A	U	19961119	9	High strength
956	US 5571166 A	U	19961105	14	Method of
957	US 5551954 A	U	19960903	11	Biodegradable
958	US 5514176 A	U	19960507	8	Pull apart
959	US 5514154 A	U	19960507	11	Expandable
960	US 5449382 A	U	19950912	9	Minimally
961	US 5441515 A	U	19950815	20	Batcheting
962	US 5411551 A	U	19950502	7	Stent assembly
963	US 5411540 A	U	19950502	7	Selective



	Document ID	KS	Issue	Da	Page	TI
1	US 5394455 A	U	19950228	16	Digit	
2	US 5713917 A	U	19980203	26	Appara	
3	US 5752522 A	U	19980519	15	Lesion	
4	US 5824040 A	U	19981020	35	Endolu	
5	US 5860923 A	U	19990118	20	Lesion	
6	US 5891192 A	U	19990406	5	Ion-in	
7	US 5902308 A	U	19990511	15	Lesion	
8	US 5902308 A	D	19990511		Body I	
9	US 5948017 A	U	19990907	20	Modula	
10	US 5957929 A	U	19990928	12	Expans	
11	US 5970119 A	U	19991019	16	Radiol	
12	US 5970119 A	D	19991019		Radiol	
13	US 5972023 A	U	19991026	23	Implar	
14	US 6010511 A	U	20000104	15	Lesion	
15	US 6078832 A	U	20000620	20	Lesion	
16	US 6084941 A	U	20000704	8	Device	
17	US 6099548 A	U	20000808	27	Appara	
18	US 6106549 A	U	20000822	21	Modula	
19	US 6187015 B1	U	20010213	12	Expans	
20	US 20010005793	U	20010628	12	Expans	
21	US 6273895 B1	U	20010814	16	Methoc	
22	US 6283991 B1	U	20010904	34	Endolu	
23	US 6287335 B1	U	20010911	102	Intrav	
24	US 6287315 B1	U	20010911	27	Appara	
25	US 20010027338	U	20011004	11	Endova	
26	US 20010047198	U	20011129	104	Intrav	
27	US 6334869 B1	U	20020101	25	Endolu	
28	US 20020026210	U	20020228	18	Endova	
29	US 20020065545	U	20020530	28	Appara	
30	US 20020068967	U	20020606	104	Intrav	
31	US 6406487 B2	U	20020618	12	Expans	
32	US 20020077634	U	20020620	28	Methoc	
33	US 20020120327	U	20020829	36	Endolu	
34	US 6451051 B2	U	20020917	100	Intrav	
35	US 20020151954	U	20021017	13	Expans	
36	US 20020165572	U	20021107	22	Emboli	
37	US 20020183629	U	20021205	11	Implar	
38	US 20020183628	U	20021205	13	Pressu	
39	US 20030004562	U	20030102	13	Endolu	
40	US 20030125790	U	20030703	12	Deploy	
41	US 6592612 B1	U	20030715	26	Methoc	
42	US 20030136417	U	20030724	25	Implar	
43	US 20030149368	U	20030807	11	Methoc	

the length of the aneurysm can be determined by reading the calibration marks 30.

Detailed Description Text - DETX (18):

Referring to FIGS. 7-11, an exemplary method for measuring the length of a vascular aneurysm in a blood vessel 54 will be described. The method will be described with reference to the catheter 10 employing the centering balloon 44 as shown in FIG. 5. As shown in FIG. 7, the guidewire 40 is initially introduced into the vessel 54 so that it passes through the aneurysm 56. The catheter 10 is then advanced along the guidewire 40 while held within the third member 50 until a proximal end 58 of the aneurysm 56 is reached. Conventional fluoroscopy procedures are employed to visualize the radiopaque markers 18, 26 and the aneurysm 56. The catheter 10 is adjusted until the radiopaque marker 18 is aligned with a target location at the proximal end 58 of the aneurysm 56. Preferably, the target location will be at about 0.5 cm to 10 cm from the aneurysm 56. Such a distance provides sufficient space for placement of a proximal end of a graft. As shown in FIG. 8, the third elongate member 50 can optionally be radially expanded or have a malecot actuated to center the catheter 10 within the vessel 54.

Detailed Description Text - DETX (24):

A further advantage of the catheter 70 is that both the diameter and the orientation of the markers 78 in the lumen can be determined. For example, an ultrasonic imaging transducer can be inserted through lumen 74 where it can be rotated to determine the diameter of the markers 78 and the distance between each of the markers 78. Ultrasound can be used with either an elastic or an inelastic balloon 76. Use of ultrasound is advantageous in providing excellent data acquisition. The resulting dimensions can then be used to construct a dimensionally significant graphical representation, such as a three dimensional wireframe model, of the markers 78. Such a model would yield the length, diameter, and radius or curvature of the body lumen and could be used in the selection of an appropriately sized prosthetic device, such as a stent graft for treating aneurysmal disease.

FileEditViewToolsWindowHelp

12: (43) (measure or) US 5752522 A | Tag: S | Doc: 3/43 (SORTED) | Format: KWIC

12: (43) (measure or) US 5752522 A | Tag: S | Doc: 3/43 (SORTED) | Format: KWIC

US 5752522 A | Tag: S | Doc: 3/43 (SORTED) | Format: KWIC

Document ID

RSC

Issue-Date

Page

Title

1US 5394455 AU 1995022816Digit

2US 5713917 AU 1998020326Appara

3US 5752522 AU 1998051915Lesion

4US 5824040 AU 1998102035Endolu

5US 5860923 AU 1999011920Lesior

6US 5891192 AU 199904065Ion-in

7US 5902308 AU 1999051115Lesior

8US 5902308 AD 19990511Body I

9US 5948017 AU 1999090720Modula

10US 5957929 AU 1999092812Expans

11US 5970119 AU 1999101916Radiol

12US 5970119 AD 19991019Radiol

13US 5972023 AU 1999102623Implar

14US 6010511 AU 2000010415Lesior

15US 6078832 AU 2000062020Lesior

16US 6084941 AU 200007048Device

17US 6099548 AU 2000080827Appara

18US 6106549 AU 2000082221Modula

19US 6187015 B1U 2001021312Expans

20US 20010005793U 2001062812Expans

21US 6273895 B1U 2001081416Method

22US 6283991 B1U 2001090434Endolu

23US 6287335 B1U 20010911102Intrav

24US 6287315 B1U 2001091127Appara

25US 20010027338U 2001100411Endova

26US 20010047198U 20011129104Intrav

27US 6334869 B1U 2002010125Endolu

28US 20020026210U 2002022818Endova

29US 20020065545U 2002053028Appara

30US 20020068967U 20020606104Intrav

31US 6406487 B2U 2002061812Expans

32US 20020077634U 2002062028Method

33US 20020120327U 2002082936Endolu

34US 6451051 B2U 20020917100Intrav

35US 20020151954U 2002101713Expans

36US 20020165572U 2002110722Emboli

37US 20020183629U 2002120511Implar

38US 20020183628U 2002120513Pressu

39US 20030004562U 2003010213Endolu

40US 20030125790U 2003070312Deploy

41US 6592612 B1U 2003071526Method

42US 20030136417U 2003072425Implar

43US 20030149368U 2003080711Method

Methods and apparatus are therefore needed for accurately measuring the cross-section of a body lumen, and in particular the diameter, circumference, and cross-sectional area of a vascular lesion. In one particular aspect, it would be desirable to provide improved methods and apparatus for the measurement of blood vessels in the region adjacent aneurysms so that the proper size of intraluminal prostheses, such as grafts and stents, can be accurately determined. It would be further desirable if such methods and apparatus were simple to use and could be used with existing fluoroscopy technology. Finally, it would be particularly desirable if such measurements could be taken without causing unnecessary stress to the diseased vessel.

Brief Summary Text - BSTX (16):

The present invention provides methods and apparatus for determining a cross-sectional dimensions of body lumens, and particularly for determining the cross-sectional area, circumference and diameter of target regions within body lumens. Body lumens amenable to the methods and apparatus of the present invention include blood vessels, the intestines, the urethra, and the like. Although suitable for the measurement of most body lumens, the present invention will find its greatest use in the measurement of vascular lesions, particularly vascular aneurysms, vascular stenoses, and the like. Advantageously, the cross-sectional dimensions of such lesions can be used to select the proper size of intraluminal prostheses, such as grafts and stents, the proper balloon for balloon angioplasty procedures, and the proper therapy for that vascular lesion.

Detailed Description Text - DETX (2):

The present invention provides methods and apparatus for determining cross-sectional dimensions, such as the internal diameter, circumference, or cross-sectional area, of a body lumen. The methods and apparatus will preferably be used to measure the cross-section of vascular lesions, and will find its greatest use in measuring the diameter of vascular aneurysms and stenoses. The methods and apparatus can also find use in measuring internal dimensions of other defects or abnormalities. Diameter and peripheral lengths provided by the present invention will be particularly useful in sizing intraluminal prostheses, such as vascular grafts or stents, that are endovascularly placed within the vessel to treat the aneurysm or other abnormality. Cross-sectional areas provided by the invention can also be used to select the proper diameter for a balloon angioplasty catheter or to size other therapeutic devices.

Detailed Description Text - DETX (11):

As shown in FIG. 2, catheter 10 has been inserted within an abnormal lumen 30 and aligned with a target region 32. The diameter of target region 32 might, for example, be needed to determine the size of an intraluminal stent to be inserted within lumen 30. Balloon 20 is shown inflated, thereby blocking a normal blood flow F. Thus the pressure and flow acting on external sensor 24 has been altered. This information is transmitted to the physician via wire

US-PAT-NO: 5824040

DOCUMENT-IDENTIFIER: US 5824040 A

TITLE: Endoluminal prostheses and therapies for highly variable body lumens

----- KWIC -----

Detailed Description Text - DETX (22):

A method of fabricating a helical stent-graft 71 will be described with reference to FIG. 5E. A series of linked diamond-shaped elements 73 are first attached to a strip of liner material 75, typically being stitched with a sewing machine. The ribbon is then wound over a mandrel 77 of the desired size, and adjacent edges of the ribbon are sewn to each other (or otherwise permanently joined). Such a method may be substantially automated and continuous, and is thus particularly beneficial for producing a large number of prostheses. The helical ~~stent-graft may optionally be cut~~ to length, but will preferably include a crown stitched stent-ring 79 for sealing and ends against a surrounding lumen when deployed therein.